# Reducing Volume Shrinkage by Low-Temperature Photopolymerization

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Received 17 March 2006; accepted 2 October 2006 DOI 10.1002/app.25758 Published online in Wiley InterScience (www.interscience.wiley.com).

**ABSTRACT:** Low-volume-shrinkage poly(triethylene glycol dimethacrylate) was made by photopolymerization at a low temperature. The final double-bond conversion and dynamic mechanical analysis indicated the optimal cure temperature to be  $-40^{\circ}$ C, at which a cured sample had less volume shrinkage than samples cured at room temperature but similar mechanical properties. © 2007 Wiley Periodicals, Inc. J Appl Polym Sci 104: 1126–1130, 2007

Key words: FT-IR; kinetics (polym.); photopolymerization

#### INTRODUCTION

Photopolymerization, a newly developed technology, has been used widely in a variety of fields such as coatings, adhesion, microlithography, and dental restoration because of advantages such as low energy consumption and fast polymerization speeds.<sup>1–5</sup> However, one of the big drawbacks of free-radical photopolymerization is volume shrinkage during the fast formation of high-density networks, which has been attributed to changes in the interatomic interactions from van der Waals forces to covalent bonds.<sup>6,7</sup> The volume shrinkage results in some failure of performance. For example, in dental restoratives, volume shrinkage causes the formation of a contraction gap between the restoration and the cavity walls and then leads to recurrent caries if cariogenic bacteria subsequently invade the gap.<sup>8,9</sup> In industry coating applications, volume shrinkage causes a reduction of adhesion between coating layers and substrates. Thus, to solve this problem, a lot of research has been undertaken in recent years, such as the synthesis of expandable monomers, ring-opening polymerization, and cationic polymerization.<sup>10–12</sup> For these polymerizable systems, the volume expands during polymerization because the release of ring strain through ring opening can compensate the volume shrinkage, which occurs because the distance between the monomer

Journal of Applied Polymer Science, Vol. 104, 1126–1130 (2007) © 2007 Wiley Periodicals, Inc.



molecules becomes close from the van der Waal distance to the covalent distance.<sup>13</sup>

Usually, photopolymerization is carried out at room temperature. Little attention has been paid to the influence of low temperatures on volume shrinkage. Research has indicated that the quantum yields of photoinitiators increase with increasing cure temperature  $(T_{cure})$ .<sup>14</sup> The double-bond conversion is reduced at low temperatures, and then the shrinkage due to the polymerization reaction is lower. Recently, research results in our group<sup>15</sup> indicated that the double-bond conversion was reduced for a system photopolymerized at a low temperature because of the vitrification of the polymer network at a very early stage of the polymerization. The free radical was trapped within the network, then the double bond could not move to approach the free radical, and the polymerization ceased at a very low double-bond conversion; however, the final conversion after the postcure was almost the same as that of a system polymerized at room temperature because the trapped free radical could continue to induce polymerization when the temperature changed from a low temperature to room temperature. The mechanical properties of the polymer film polymerized at a low temperature were almost the same as those of the film polymerized at room temperature. When the temperature was increased to room temperature, the volume of the polymer film expanded, and this counteracted the shrinkage due to the polymerization reaction. Then, the volume shrinkage of the polymer film polymerized at a low temperature was lower than that of the film polymerized at room temperature.

In this study, triethylene glycol dimethacrylate (TEGDMA) was photopolymerized at different  $T_{\text{cure}}$  values (from -75 to  $20^{\circ}$ C), the double-bond conver-

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sion was measured by Fourier transform infrared (FTIR), the loss tangent (tan  $\delta$ ) and the glass-transition temperature ( $T_g$ ) were recorded by dynamic mechanical analysis (DMA), and the volume shrinkage was measured by the pycnometric method.

#### **EXPERIMENTAL**

The monomer TEGDMA (SR205) was donated by Sartomer Co., Inc. (Warrington, PA). The photoinitiator 1-hydroxycyclohexyl phenyl ketone (HCPK) was supplied by High-Tech Insight Co., Ltd. (Beijing, China). These materials were used without further purification. The basic formulation of the photopolymerization system was the monomer and 0.5 wt % HCPK. After the addition of the photoinitiator, the photopolymerization system was stirred until HCPK was dissolved completely.

For the investigation of the double-bond conversion, the sample was injected into a mold of a uniform size (76  $\times$  26  $\times$  0.5 mm<sup>3</sup>) and isothermally cured under a UV-light source (model 100 UV, Rolence, Taiwan) for 400 s with a light intensity of 2735 mW/cm<sup>2</sup> (UV meter, Honle, Grafelfing, Germany). The isothermal photopolymerization (at temperatures ranging from -75 to  $20^{\circ}$ C) was performed with a PSL1800 cooler (Eyela, Tokyo, Japan; ethanol was used as the cooler medium). The double-bond conversion was monitored by near-infrared (Nicolet 5700 FTIR, Nicolet Instrument, Madison, WI); the change in the absorption area from 6207 to 6124 cm<sup>-1</sup> was measured before and after UV irradiation. The initial conversion was calculated with eq. (1). For the postcure reaction, the samples were taken from the cooler and put into the FTIR apparatus at room temperature to measure the change in the absorption area from 6207 to 6124 cm<sup>-1</sup> at different times. The postcure conversion was calculated with eq. (2). The final double-bond conversion was defined as the double-bond conversion after the postcure process was finished:

Initial conversion (%) =  $(1 - S_2/S_1) \times 100$  (1)

Postcure conversion (%) =  $(1 - S_n/S_1) \times 100$  (2)

where  $S_1$  is the =CH peak area before UV irradiation,  $S_2$  is the =CH peak area after UV irradiation, and  $S_n$  is the =CH peak area during the postcure.

For DMA, samples of a uniform size of  $35 \times 7 \times 0.5 \text{ mm}^3$  were prepared, and the measurements were performed with a DMTA-V dynamic mechanical analyzer (Rheometric, Scientific Inc., Piscataway, NJ) in the range of -60 to  $200^{\circ}$ C with a ramping rate of  $5^{\circ}$ C/min with an extension mode. Tan  $\delta$  was recorded as a function of temperature.  $T_g$  was taken to be the maximum of the tan  $\delta$ /temperature curve. For each

system, three repeat experiments were performed. The densities of the monomer and polymer were measured by the pycnometric method.

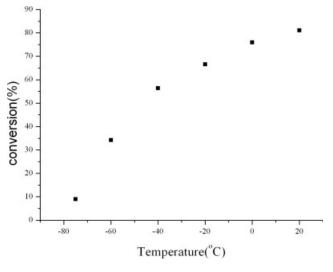
### **RESULTS AND DISCUSSION**

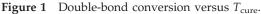
#### Effect of $T_{cure}$ on the double-bond conversion

The photopolymerization system of TEGDMA and 0.5 wt % HCPK was cured by UV radiation at different  $T_{\text{cure}}$  values ranging from -75 to 20°C; the double-bond conversions are shown in Figure 1 and Table I. Figure 1 illustrates that the double-bond conversion decreased steadily with the drop in  $T_{\text{cure}}$ . When  $T_{\text{cure}}$  was  $-75^{\circ}$ C, the initial double-bond conversion was 9%; when  $T_{\text{cure}}$  increased to 20°C, the initial double-bond conversion (81.7%) was 9 times higher than that of the sample cured at  $-75^{\circ}$ C.

During the process of free-radical polymerization, a microgel was formed at very early stages of polymerization, thus reducing the mobility of the molecular segments of the reacting systems. Once  $T_g$  approached  $T_{\text{cure}}$ , the system vitrified, so polymerization ceased.<sup>16–19</sup> The difference between  $T_{\text{cure}}$  and  $T_g$  had an important effect on the vitrification of the system. When the formulation was cured at a lower temperature, the difference between  $T_{\text{cure}}$  and  $T_g$  was less, and the formulation vitrified at an earlier stage, so the double-bond conversion at a lower  $T_{\text{cure}}$  was low.

Moreover, the viscosity of the formulation was also a crucial factor for the double-bond conversion. Scherzer and Decker<sup>20</sup> found that the double-bond conversion strongly increased with decreasing viscosity because of the rise of  $T_{\text{cure}}$ , which led to a strong increase in the molecular diffusion and reactivity. Thus, a drop in  $T_{\text{cure}}$  led to an increase in the





Journal of Applied Polymer Science DOI 10.1002/app

Data for the Samples Cured at Different Temperatures						
	$T_{\text{cure}}$ (°C)					
	20	0	-20	-40	-60	-75
Conversion after the photocuring (%)	81.7	75	66.8	56.6	34.4	9
Conversion after the dark reaction (%)	84.5	85.3	82.2	81.5	63.6	19.9
$T_g$ (°C)	146	146	145	146	65	-1
Density of the monomer (g/mL)	1.08	1.11	1.15	1.18	1.22	1.24
Density of the polymer $(g/mL)$	1.24	1.25	1.26	1.24	1.25	1.22
Volume shrinkage (%)	12.9	11.2	8.7	4.8	2.4	-1.6

 TABLE I

 Data for the Samples Cured at Different Temperatures

viscosity and hence a decrease in the double-bond conversion.

#### Influence of $T_{\text{cure}}$ on the dark reaction

After being cured at different temperatures, the samples were put in the dark at room temperature to perform the dark reaction (Fig. 2 and Table I). Figure 2 illustrates that ascending trend of the postcure curves was much more striking for the sample cured at lower  $T_{cure}$ . As the temperature rose from a low temperature to room temperature, the trapped radical was released from physical crosslinking crystallinity, and the double bond was more moveable. Therefore, the double bond could approach the free radical, and the polymerization process occurred again. The double-bond conversion increased, and finally a highly crosslinked network formed; no more double bonds could approach any free radicals, and the polymerization process was finished.

Figure 2 also shows that, after 6 h of the dark reaction, the final conversions of the samples cured at different temperatures ranging from -40 to  $20^{\circ}$ C were almost the same (ca. 83%; Table I). This result agrees with the findings of Cook et al.<sup>17</sup> and Ziaee

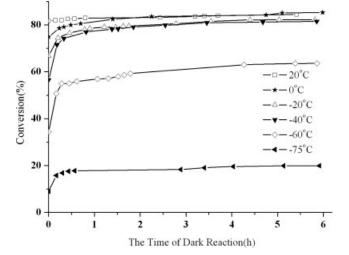


Figure 2 Postcure curves of TEGDMA cured at different temperatures.

and Palmese,<sup>21</sup> who demonstrated that the final conversion of vinyl double bonds after postcuring was the same in samples cured at temperatures ranging from -10 to 90°C. However, the final conversion of samples cured at -75 (19.9%) and -60°C (63.6%) was much less than that of samples cured at temperatures ranging from -40 to 20°C (Table I). This might be because the number of total free radicals generated, such as reactive fragments of the initiator and chain radicals, was very low at such low temperatures; on the other hand, the trapped free radical might gradually have lost its reactivity during the postcuring process, so the final conversion was lower.

## DMA

After the postcure was completed, the mechanical properties of samples cured at different temperatures were measured with the DMTA-V. The effect of  $T_{\text{cure}}$  on tan  $\delta$  is shown in Figure 3, which illustrates that the tan  $\delta$  curves of these samples cured at -40, -20, 0, and  $20^{\circ}$ C were very similar, but the profiles of tan  $\delta$  of those samples cured at -60 and  $-75^{\circ}$ C were much lower than those of the samples cured at -40, -20, 0, and  $20^{\circ}$ C. At the same time, the data in Table I indicate that the  $T_g$  values of the

 $\begin{array}{c} 0.25 \\ 0.20 \\ 0.15 \\ 0.15 \\ 0.05 \\ 0.00 \\ -50 \\ 0 \\ \end{array}$ 

Figure 3 Tan  $\delta$ /temperature curves of samples cured at different temperatures.

samples cured at -40, -20, 0, and  $20^{\circ}$ C were almost the same (145°C) and much higher than those of the samples cured at -60 and  $-75^{\circ}$ C. A number of studies have demonstrated that  $T_g$  of a photocured resin increases with the final conversion. <sup>16,17,23,24</sup> These are comparable to previous results for double-bond conversion. The final double-bond conversions of samples cured at -40, -20, 0, and  $20^{\circ}$ C were around 83%, which was higher than those of samples cured at -60 (63.6%) and  $-75^{\circ}$ C (19.9%).

#### Volume shrinkage

Calculation of the density of TEGDMA at different temperatures

Because it was difficult to get credible experimental data for the density of TEGDMA at a low temperature, the specific density had to be calculated by some empirical equations. First, we estimated some thermodynamic critical constants with the Lydersen method revised by Joback,<sup>25</sup> which could calculate them accurately and is applied widely in some fields. The equations of the Lydersen method are as follows:

$$T_b = 198 + \sum \Delta T_b \tag{3}$$

$$T_{c} = \frac{T_{b}}{0.584 + 0.965 \sum \Delta t - \left(\sum \Delta t\right)^{2}}$$
(4)

$$p_c = \frac{0.1}{\left(0.113 + 0.0032N - \sum \Delta p\right)^2} \tag{5}$$

where  $T_b$  is the boiling temperature at the normal pressure;  $T_c$  is the critical temperature;  $p_c$  is the critical pressure;  $\Delta T_b$ ,  $\Delta t$ , and  $\Delta p$  are the parameters of the summation of the contributions of all groups; and N is the number of atoms of TEGDMA. These expressions could be used to estimate  $T_b$  [eq. (3)],  $T_c$  [eq. (4)], and  $p_c$  [eq. (5)].

Then, we estimated the densities of TEGDMA at different temperatures with the Rackett equations revised by Spencer and Danner,<sup>26,27</sup> which were applied to estimate the density of the saturated liquid ( $\rho_s$ ). The Rackett equations are shown as follows:

$$V_s = \frac{RT_c(Z_r)^k}{p_c} \tag{6}$$

$$k = 1 + (1 - T_r)^{2/7}$$
 (7)

$$\rho_s = \frac{M}{V_s} \tag{8}$$

$$T_r = \frac{T}{T_c} \tag{9}$$

where  $V_s$  is the molar volume of the saturated liquid,  $Z_r$  is the characteristic constant of TEGDMA, k is the index of  $Z_r$ ,  $T_r$  is the ratio of the given temperature to  $T_c$ , R is the gas constant, and Mis mass. The density of TEGDMA at 20°C was measured, and  $Z_r$ was calculated with these equations; then, the densities of TEGDMA at different temperatures could be calculated with the Rackett equations. The calculated values are shown in Table I.

Calculation of the volume shrinkage

All the samples for volume-shrinkage measurements were set at room temperature to complete the dark reaction after they were polymerized at different temperatures. Then, the volume shrinkage of the samples was calculated with the following expression:<sup>9,28</sup>

Shrinkage (%) = 
$$\left(1 - \frac{d_{\text{uncured}}}{d_{\text{cured}}}\right) \times 100$$
 (10)

where  $d_{\text{uncured}}$  is the density of the monomer at  $T_{\text{cure}}$ and  $d_{\text{cured}}$  is the density of the polymer at room temperature (measured by the pycnometric method).<sup>26</sup> The values of the volume shrinkage are shown in Table I and indicate that the volume shrinkage decreased with the drop in  $T_{\text{cure}}$  and became negative when  $T_{\text{cure}}$  was  $-75^{\circ}$ C.

In eq. (10), the volume shrinkage is proportional to the value of  $d_{\text{uncured}}$ , which represents the numerator related to  $T_{\text{cure}}$ . When  $T_{\text{cure}}$  is lower,  $d_{\text{uncured}}$  becomes bigger, and so the volume shrinkage is less. This is a major reason for the results. Besides, the volume shrinkage is inversely proportional to the denominator,  $d_{\text{cured}}$ , which is measured at room temperature and is related to the final conversion of the completely postcured samples. The final conversions of the samples cured at different temperatures ranging from -40 to  $20^{\circ}$ C were almost the same and much higher than those of the samples cured at -60 and  $-75^{\circ}$ C (Table I). Therefore, the lower final conversion was also a reason that the volume shrinkage decreased.

#### CONCLUSIONS

Near-infrared was used to investigate the doublebond conversion of TEGDMA cured at temperature ranging from -75 to 20°C. The double-bond conversion decreased steadily with the drop in  $T_{\text{cure}}$ ; however, the final conversion of a sample cured at a lower temperature increased much more dramatically after the postcure reaction.

Although the volume shrinkage decreased with decreasing  $T_{\text{cure}}$ , the mechanical properties of samples cured at -40, -20, 0, and  $20^{\circ}\text{C}$  were much better than those of samples cured at -60 and  $-75^{\circ}\text{C}$ .

The optimal  $T_{\text{cure}}$  value was found at  $-40^{\circ}$ C, at which a cured sample had less volume shrinkage than a sample cured at room temperature but similar mechanical properties.

#### References

- 1. Fouassier, J. P.; Rabek, J. F. Radiation Curing in Polymer Science and Technology; Elsevier: London, 1993.
- 2. Fouassier, J. P. Photoinitiator, Photopolymerization and Photocuring; Hanser: Munich, 1995.
- 3. Decker, C. Macromol Rapid Commun 2002, 23, 1067.
- 4. Decker, C. Prog Polym Sci 1996, 21, 593.
- 5. Andrzejewska, E. Prog Polym Sci 2001, 26, 605.
- Cook, W. D.; Forrest, M.; Goodwin, A. A. Dent Mater 1999, 15, 447.
- 7. Rueggeberg, F.; Tamareselvy, K. Dent Mater 1995, 11, 265.
- 8. Condon, J. R.; Ferracane, J. L. Biomaterials 2002, 23, 3807.
- 9. Nie, J.; Rabek, J. F.; Lindén, L. Å. Polym Int 1999, 48, 129.
- 10. Cho, J. D.; Hong, J. W. J Appl Polym Sci 2004, 93, 1473.
- 11. Nie, J.; Bowman, C. N. Biomaterials 2002, 23, 1221.

- Lu, H.; Stansbury, J. W.; Nie, J.; Berchtold, K. A.; Bowman, C. N. Biomaterials 2005, 26, 1329.
- 13. Endo, T.; Sanda, F. Macromol Symp 2000, 159, 1.
- Stevenson, K. L.; Papadantonakis, G. A.; Le Breton, P. R. J Photochem Photobiol A 2000, 133, 159.
- 15. Lu, B.; Nie, J. Photogr Sci Photochem 2005, 23, 321.
- 16. Lecamp, L.; Youssef, B.; Bunel, C.; Lebaudy, P. Polymer 1997, 40, 1403.
- 17. Scott, T. F.; Cook, W. D.; Forsythe, J. S. Polymer 2002, 43, 5839.
- 18. Cook, W. D. Polymer 1992, 33, 2152.
- 19. Cook, W. D. J Polym Sci Part A: Polym Chem 1993, 31, 1053.
- 20. Scherzer, T.; Decker, U. Polymer 2000, 41, 7681.
- 21. Ziaee, S.; Palmese, G. R. J Polym Sci Part B: Polym Phys 1999, 37, 725.
- 22. Wisanrakkit, G.; Gillham, J. K. J Appl Polym Sci 1990, 41, 2885.
- 23. Cook, W. D.; Simon, G. P.; Burchill, P. J.; Lau, M.; Fitch, T. J. J Appl Polym Sci 1997, 64, 769.
- 24. Wise, C. W.; Cook, W. D.; Goodwin, A. A. Polymer 1997, 38, 3251.
- 25. Reid, R. C.; Praushitz, J. M. The Properties of Gases and Liquids, 4th ed.; McGraw-Hill: New York, 1987.
- 26. Rackett, H. G. J Chem Eng Data 1970, 15, 514.
- 27. Spencer, C. F.; Danner, R. P. J Chem Eng Data 1972, 17, 236.
- 28. Puckett, A. D.; Smith, R. J Prosthet Dent 1992, 58, 56.